AMENDMENTS TO THE CLAIMS

This listing of claims will replace all prior versions and listings of claims in the application:

LISTING OF CLAIMS:

- (currently amended) An in vitro method for the production of a homologous heart valve, comprising the steps of:
 - a) providing a biodegradable support comprising a broad edge,
 - colonizing the support with homologous fibroblast or myofibroblast cells
 or a combination thereof to form a connective tissue matrix,
 - optionally colonizing the connective tissue matrix with endothelial cells,
 and
 - fixing the connective tissue matrix to a non-degradable or poorly-slowly degradable frame construction,

wherein, before or after the fixing of the frame construction, the connective tissue matrix optionally colonized with endothelial cells is introduced into a pulsatile flow chamber in which it can be exposed to increasing flow rates, wherein the flow rate is increased continuously or discontinuously, wherein the broad edge is a suture ring, wherein the biodegradable support begins degrading at least 8 days post colonization and is completely degraded no later than 3 months after colonization, and wherein the poorly slowly degradable frame does not degrade prior to a year after colonization.

(currently amended) An in vitro method for the production of a homologous heart valve, comprising the following steps:

- a) providing a biodegradable support which is firmly connected to a
 non-degradable or poorlyslowly degradable frame construction, wherein
 the biodegradable support comprises a broad edge, and wherein the broad
 edge is a suture ring,
- colonizing the support with homologous fibroblast or myofibroblast cells or a combination thereof to form a connective tissue matrix,
- c) optionally colonizing the connective tissue matrix with endothelial cells,
- d) introducing the frame construction with the connective tissue matrix connected thereto into a pulsatile flow chamber in which it can be exposed to increasing flow rates, and
- e) continuously or discontinuously increasing of the flow rate,

wherein the biodegradable support begins degrading at least 8 days post colonization and is completely degraded no later than 3 months after colonization and wherein the poorly-slowly degradable frame does not degrade prior to a year after colonization.

- (previously presented) The method according to claims 1 or 2, wherein the biodegradable support comprises a biodegradable polymer matrix or an acellular biological matrix.
- 4. (previously presented) The method of claim 3, wherein the support comprises a polyglycolic acid (PGA), polylactic acid (PLA), polyhydroxyalkanoate (PHA), poly-4-hydroxybutyrate (P4HB) or a mixture of two or more of these polymers.

- 5. (previously presented) The method according to claims 1 or 2, wherein the support has a polymer density of 40 to 120 mg/cm^3 .
- 6. (previously presented) The method according to claims 1 or 2, wherein the support comprises a porous polymer having a pore size of 80 to 240 μm .
- 7. (previously presented) The method according to claims 1 or 2, wherein the fibers of the support have a diameter of 6 to 20 μm .
- (previously presented) The method of claim 3, wherein the support comprises an
 acellular connective tissue framework of an animal or human heart valve.
- (previously presented) The method according to claims 1 or 2, wherein the step of colonization with fibroblast or myofibroblasts cells or a combination thereof repeated 3 to 14 times.
- 10. (previously presented) The method according to claims 1 or 2, wherein approximately 10^5 to 6×10^8 fibroblast or myofibroblast cells or a combination thereof are employed per square centimeter of support.
- 11. (previously presented) The method according to claims 1 or 2, wherein the step of colonization with endothelial cells is repeated 3 to 14 times.

- 12. (previously presented) The method according to claims 1 or 2, wherein approximately 10^5 to 5×10^8 endothelial cells are employed per square centimeter of support.
- (previously presented) The method according to claims 1 or 2, wherein the cells are human cells.
- 14. (previously presented) The method according to claims 1 or 2, wherein the cells are autologous cells.
- 15. (previously presented) The method according to claims 1 or 2, wherein the frame construction comprises a biocompatible material.
 - 16. (cancelled).
- 17. (previously presented) The method according to claims 1 or 2, wherein the support is fixed to the frame construction by means of conventional suturing, fibrin adhesive, or a combination thereof.
- 18. (previously presented) The method according to claims 1 or 2, wherein flow rates of 5 ml/min to $8{,}000$ ml/min are established in the pulsatile flow chamber.
- 19. (previously presented) The method according to claims 1 or 2, wherein the flow rate is increased over a period of 1 week to 12 weeks.

- (previously presented) The method according to claims 1 or 2, wherein the initial flow rate is 50 to 100 ml/min.
- (previously presented) The method according to claims 1 or 2, wherein the initial pulse frequency is 5 to 10 pulses/min.
- (previously presented) The method according to claims 1 or 2, wherein the flow rate is increased to 5,000 ml/min.
- (previously presented) The method according to claims 1 or 2, wherein the pulse frequency is increased to 180 pulses/min.
- 24. (previously presented) The method according to claims 1 or 2, wherein systemic pressures of 10 to 240 mm Hg are established in the pulsatile flow chamber.
- 25. (previously presented) An autologous heart valve that has been produced by the method according to claims 1 or 2.
- 26. (currently amended) An autologous heart valve having a connective tissue inner structure surrounded by an endothelial cell layer, wherein the connective tissue inner structure is fixed to a non-degradable or slowly degradable frame construction, wherein the frame construction comprises a broad edge wherein the broad edge is a suture ring, wherein the biodegradable support begins degrading at least 8 days post colonization with the endothelial cell

layer and is completely degraded no later than 3 months after colonization with the endothelial cell layer and wherein the poorly-slowly degradable frame does not degrade prior to a year after colonization with the endothelial cell layer.

- 27. (previously presented) The autologous heart valve according to claim 26, wherein a collagen density of 20 to 60 % exists in the connective tissue inner structure.
- 28. (previously presented) The autologous heart valve according to claim 27, wherein the heart valve withstands the flow conditions in the human heart.